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# **Pysiology Documentation**

*Release 0.0.9 - Beta version*

**Giulio Gabrieli**

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Version: 0.0.9.4

[Github](#) [Pypi](#)



# CHAPTER 1

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## Introduction

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PySiology is a python package developed with the intent of make physiological analysis accessible to researchers worldwide.

PySiology is a tool designed with novice users in mind, and it provides a simple way to estimate features from ECG, EMG and EDA signals. Features estimation is done chaining functions, and for each method default value are provided. This allows for a fast estimation of more than 50 features. Furthermore, PySiology provides tutorials that allows not only to learn how to use the package, but also the methodologies behind its modules.

Expert users can customize each estimation parameter, add their own and share their results with other users.





To install Pysiology on your machines, you can use pip or install it manually using the setup.py file. Since Pysiology is based on Python, you will need Python installed on your machine as well. This will install all the required dependencies as well.

## 2.1 Download and Installation

### 2.1.1 Using pip (suggested method)

Open a terminal and type:

```
pip install pysiology
```

### 2.1.2 Using setup.py

Download or clone the repository, extract it and open a terminal inside the root of the project. Then type:

```
python setup.py install
```

## 2.2 Testing

To test the installation of the package, run the file test.py or:

```
import pysiology
print(pysiology.__version__)
```

If everything went good, you should see the installed version.



### 3.1 Electrocardiography analysis module

```
electrocardiography.analyzeECG(rawECGSignal, samplerate, preprocessing=True, highpass=0.5,  
                                lowpass=2.5, min_dist=500, peakThresh=0.3, PeakTreshAbs=False, ibi=True, bpm=True, sdn=True, sdsd=True,  
                                rmssd=True, pnn50=True, pnn20=True, pnn50pnn20=True,  
                                freqAnalysis=True, freqAnalysisFiltered=True)
```

This is a simple entrypoint for ECG analysis.

You can use this function as model for your analysis or to extrapolate several features from an ECG signal.

You can specify which features to evaluate or to exclude, as well as cutoff for frequencies and filter.

#### Parameters

- **data** (*list*) – ECG signal
- **samplerate** (*int*) – samplerate of the signal in Hz
- **preprocessing** (*boolean*) – whether to perform a simple preprocessing of the signal automatically
- **highpass** (*boolean*) – cutoff frequency for the high pass filter
- **lowpass** (*boolean*) – cutoff frequency for the low pass filter
- **min\_dist** (*int*) – minimum distance between peaks in ms. Used for peak detection
- **peakThresh** (*float*) – Normalized threshold. Only the peaks with amplitude higher than the threshold will be detected by the peak detection utils
- **PeakTreshAbs** (*boolean*) – If True, the peakThresh value will be interpreted as an absolute value, instead of a normalized threshold.
- **ibi** (*boolean*) – whether or not to perform the IBI analysis
- **bpm** (*boolean*) – whether or not to perform the BPM analysis

- **sdnn** (*boolean*) – whether or not to perform the sdnn analysis
- **sdsd** (*boolean*) – whether or not to perform the sdsd analysis
- **rmssd** (*boolean*) – whether or not to perform the rmssd analysis
- **pnn50** (*boolean*) – whether or not to perform the pNN50 analysis
- **pnn20** (*boolean*) – whether or not to perform the pNN20 analysis
- **pnn50pnn20** (*boolean*) – whether or not to perform the pNN50 on pNN20 ratio analysis
- **freqAnalysis** (*boolean*) – whether or not to perform a frequency analysis analysis
- **freqAnalysisFiltered** (*boolean*) – whether or not to perform a frequency analysis automatically filtering the signal

**Returns** a dictionary containing the results of the ECG analysis

**Return type** list

electrocardiography.**butter\_highpass** (*cutoff, fs, order=5*)

This functions generates a hignpass butter filter

**Parameters**

- **cutoff** (*float*) – cutoff frequency
- **cutoff** – cutoff frequency
- **fs** (*float*) – samplerate of the signal
- **order** (*int*) – order of the Butter Filter

**Returns** butter highpass filter

**Return type** list

electrocardiography.**butter\_highpass\_filter** (*data, cutoff, fs, order*)

This functions apply a butter highpass filter to a signal

**Parameters**

- **data** (*list*) – ECG signal
- **cutoff** (*float*) – cutoff frequency
- **cutoff** – cutoff frequency
- **fs** (*float*) – samplerate of the signal
- **order** (*int*) – order of the Butter Filter

**Returns** highpass filtered ECG signal

**Return type** list

electrocardiography.**butter\_lowpass** (*cutoff, fs, order=5*)

This functions generates a lowpass butter filter

**Parameters**

- **cutoff** (*float*) – cutoff frequency
- **cutoff** – cutoff frequency
- **fs** (*float*) – samplerate of the signal
- **order** (*int*) – order of the Butter Filter

**Returns** butter lowpass filter

**Return type** list

electrocardiography.**butter\_lowpass\_filter**(*data, cutoff, fs, order*)

This functions apply a butter lowpass filter to a signal

**Parameters**

- **data** (*list*) – ECG signal
- **cutoff** (*float*) – cutoff frequency
- **cutoff** – cutoff frequency
- **fs** (*float*) – samplerate of the signal
- **order** (*int*) – order of the Butter Filter

**Returns** lowpass filtered ECG signal

**Return type** list

electrocardiography.**getBPM**(*npeaks, nsample, samplerate*)

This function returns the BPM of a discrete heart signal.

Input: number of peaks of the ECG signal, number of samples, samplerate of the signal

Output: BPM

**Parameters**

- **npeak** (*int*) – number of peaks of the ECG signal
- **nsample** (*int*) – number of samples of the ECG signal
- **samplerate** (*int*) – samplerate of the signal in Hz

**Returns** BPM of the ECG signal

**Return type** float

electrocardiography.**getFrequencies**(*rawECGSignal, samplerate, llc=0.04, ulc=0.15, lhc=0.15, uhc=0.4, lvlc=0.0033, hvlc=0.04*)

This functions returns the sum of the PSD of low Frequencies, high frequencies and very low frequencies.

Default Values have been adapted from: Blood, J. D., Wu, J., Chaplin, T. M., Hommer, R., Vazquez, L., Rutherford, H. J., ... & Crowley, M. J. (2015). The variable heart: high frequency and very low frequency correlates of depressive symptoms in children and adolescents. *Journal of affective disorders*, 186, 119-126.

It returns a dictionary with the values for high, low and very low frequencies

**Parameters**

- **rawECGSignal** (*list*) – raw ECG signal
- **samplerate** (*int*) – samplerate of the ECG signal
- **llc** (*float*) – lower cutoff of low frequencies
- **ulc** (*float*) – upper cutoff of low frequencies
- **lhc** (*float*) – lower cutoff of high frequencies
- **uhc** (*float*) – high cutoff of high frequencies
- **lvlc** (*float*) – lower cutoff of very low frequencies
- **uvlc** (*float*) – upper cutoff of very low frequencies

**Returns** a dictionary containing the results of the frequency analysis

**Return type** dictionary

`electrocardiography.getIBI` (*peaks, samplerate*)

This function returns the IBI of a discrete heart signal.

Input: peaks and samplerate of the ECG signal

Output: IBI in ms

**Parameters**

- **peaks** (*list*) – list of peaks of the ECG signal
- **samplerate** (*int*) – samplerate of the signal in Hz

**Returns** the mean IBI of the ECG signal

**Return type** IBI (in ms) as float value

`electrocardiography.getPNN20` (*peaks, samplerate*)

This functions evaluate pNN20, the proportion of differences greater than 20ms.

Input: peaks of the ECG signal,samplerate of the signal

Output: proportion of number of pairs of successive peaks that diffear by more than 20ms

**Parameters**

- **peaks** (*list*) – list of peaks in the ECG signal
- **samplerate** (*int*) – samplerate of the signal in Hz

**Returns** the pNN20 of the ECG signal

**Return type** float

`electrocardiography.getPNN50` (*peaks, samplerate*)

This functions evaluate pNN50, the proportion of differences greater than 50ms.

Input: peaks of the ECG signal,samplerate of the signal

Output: proportion of number of pairs of successive peaks that diffear by more than 50ms

**Parameters**

- **peaks** (*list*) – list of peaks in the ECG signal
- **samplerate** (*int*) – samplerate of the signal in Hz

**Returns** the pNN50 of the ECG signal

**Return type** float

`electrocardiography.getRMSSD` (*peaks, samplerate*)

This functions evaluate the root mean square of successive differences between adjacent R-R intervals.

$RMSSD = \sqrt{(1 / (N - 1)) * \sum(i=1 \rightarrow N)(RRdiff\ i - \text{mean}(RRdiff))^{*2}}$

Input: peaks of the ECG signal,samplerate of the signal.

Output: the root mean square of successive differences between adjacent R-R intervals.

**Parameters**

- **peaks** (*list*) – list of peaks in the ECG signal
- **samplerate** (*int*) – samplerate of the signal in Hz

**Returns** the RMSSD of the ECG signal

**Return type** float

`electrocardiography.getSDNN` (*peaks*, *samplerate*)

This functions evaluate the standard deviation of intervals between heartbeats. It is often calculated over 24h period, or over short peridos of 5 mins.

SDNN reflects all the cyclic components responsible for variability in the period of recording, therefore it represents total variability

$SDNN = \sqrt{((1/N-1) * \sum(i=1 \rightarrow N)(rri - rrmean)^2)}$

Input: peaks of the ECG signal,samplerate of the signal

Output: standard deviations of Intervals between heartbeats.

**Parameters**

- **peaks** (*list*) – list of peaks in the ECG signal
- **samplerate** (*int*) – samplerate of the signal in Hz

**Returns** the SDNN of the ECG signal

**Return type** float

`electrocardiography.getSDSD` (*peaks*, *samplerate*)

This functions evaluate the the standard deviation of successive differences between adjacent R-R intervals.

$SDSD: \sqrt{((1 / (N - 1)) * \sum(i=1 \rightarrow N)(RR i - \text{mean}(RR))^2)}$

Input: peaks of the ECG signal,samplerate of the signal

Output: the standard deviation of successive differences between adjacent R-R intervals

**Parameters**

- **peaks** (*list*) – list of peaks in the ECG signal
- **samplerate** (*int*) – samplerate of the signal in Hz

**Returns** the SDSD of the ECG signal

**Return type** float

## 3.2 Electrodermal Activity analysis module

`electrodermalactivity.GSRSCRFeaturesExtraction` (*filteredGSRSignal*, *samplerate*, *peak*)

This functions extract GSR SCR features: [http://eda-explorer.media.mit.edu/static/SCR\\_withFeatures.png](http://eda-explorer.media.mit.edu/static/SCR_withFeatures.png)

• **Input:**

- rawGSRSignal: filtered GSR Signal as list
- samplerate: samplerate of the signak§
- peak: list of peaks [peakStart, max, peakend]

• **Output:**

- dict: {riseTime,Amplitude,EDAatApex,DecayTime (50%),SCRWidth (50%)}

**Parameters**

- **rawGSRSignal** (*list*) – raw GSR Signal

- **samplerate** (*int*) – samplerate of the GSR signal in Hz
- **peak** (*list*) – a list containing the peak onset, max and offset indexes (as returned by the function `findPeakOnsetAndOffset`)

**Returns** a dictionary with the results of the extracted features

**Return type** dict

`electrodermalactivity.analyzeGSR` (*rawGSRSignal*, *samplerate*, *preprocessing=True*, *lowpass=1*, *highpass=0.05*, *phasic\_seconds=10*)

Entry point for gsr analysis. Signal is filtered and downsampled, then a phasic filter is applied

• **Input:**

- `rawGSRSignal` = gsr signal as list
- `samplerate` = samplerate of the signal
- `preprocessing` = whether to perform or not a preprocessing of the signal
- `lowpass` = cutoff for lowpass filter
- `highpass` = cutoff for highpass filter

• **Output:**

- dictionary with all the results

**Parameters**

- **rawGSRSignal** (*list*) – raw GSR Signal
- **samplerate** (*int*) – samplerate of the GSR signal in Hz
- **preprocessing** (*true*) – whether to perform or not an automatic preprocessing of the signal
- **lowpass** (*float*) – cutoff frequency for the lowpass filter
- **highpass** (*float*) – cutoff frequency for the highpass filter

**Returns** a dictionary with the results of the automatic GSR analysis

**Return type** dict

`electrodermalactivity.butter_highpass` (*cutoff*, *fs*, *order=5*)

This function generates a highpass butter filter

**Parameters**

- **cutoff** (*float*) – cutoff frequency
- **cutoff** – cutoff frequency
- **fs** (*float*) – samplerate of the signal
- **order** (*int*) – order of the Butter Filter

**Returns** butter highpass filter

**Return type** list

`electrodermalactivity.butter_highpass_filter` (*data*, *cutoff*, *fs*, *order*)

This function applies a butter highpass filter to a signal

**Parameters**



- **data** (*list*) – ECG signal
- **cutoff** (*float*) – cutoff frequency
- **cutoff** – cutoff frequency
- **fs** (*float*) – samplerate of the signal
- **order** (*int*) – order of the Butter Filter

**Returns** highpass filtered ECG signal

**Return type** list

electrodermalactivity.**butter\_lowpass** (*cutoff, fs, order=5*)

This functions generates a lowpass butter filter

**Parameters**

- **cutoff** (*float*) – cutoff frequency
- **cutoff** – cutoff frequency
- **fs** (*float*) – samplerate of the signal
- **order** (*int*) – order of the Butter Filter

**Returns** butter lowpass filter

**Return type** list

electrodermalactivity.**butter\_lowpass\_filter** (*data, cutoff, fs, order*)

This functions apply a butter lowpass filter to a signal

**Parameters**

- **data** (*list*) – ECG signal
- **cutoff** (*float*) – cutoff frequency
- **cutoff** – cutoff frequency
- **fs** (*float*) – samplerate of the signal
- **order** (*int*) – order of the Butter Filter

**Returns** lowpass filtered ECG signal

**Return type** list

electrodermalactivity.**findPeakOnsetAndOffset** (*rawGSRSignal, onset=0.01, offset=0*)

This functions finds the peaks of a GSR signal

• **Input:**

- rawGSRSignal = GSR signal as list
- onset = onset for Peak Detection (uS)
- offset = offset for Peak Detection (uS)

• **Output:**

- multi dimensional list, [onsetIndex,maxIndex,offsetIndex] x nPeaks

**Parameters**

- **rawGSRSignal** (*list*) – GSR Signal to analyze
- **onset** (*float*) – onset value for peak detection (in uS)

- **offset** (*float*) – onset value for peak detection (in uS)

**Returns** list of the peaks in the signal

**Return type** float

`electrodermalactivity.getPhasicAndTonic` (*rawGSRSignal*, *samplerate*, *seconds=4*)

This function returns the phasic and tonic components of a signal.

• **Input:**

- *rawGSRSignal* = gsr signal as list
- *samplerate* = samplerate of the signal
- *seconds* = number of seconds before and after each timepoint to use in order to compute the filtered value

• **Output:**

- List containing the phasic and tonic components

**Parameters**

- **rawGSRSignal** (*list*) – raw GSR Signal
- **samplerate** (*int*) – samplerate of the GSR signal in Hz
- **seconds** – seconds to use to apply the phasic filter
- **seconds** – int

**Returns** phasic and tonic signals

**Return type** list

`electrodermalactivity.phasicGSRFilter` (*rawGSRSignal*, *samplerate*, *seconds=4*)

Apply a phasic filter to the signal, with +/- X seconds from each sample. Default is 4 seconds

• **Input:**

- *rawGSRSignal* = gsr signal as list
- *samplerate* = samplerate of the signal
- *seconds* = number of seconds before and after each timepoint to use in order to compute the filtered value

• **Output:**

- phasic signal

**Parameters**

- **rawGSRSignal** (*list*) – raw GSR Signal
- **samplerate** (*int*) – samplerate of the GSR signal in Hz
- **seconds** – seconds to use to apply the phasic filter
- **seconds** – int

**Returns** filtered signal

**Return type** list

`electrodermalactivity.tonicGSRFilter` (*rawGSRSignal*, *samplerate*, *seconds=4*)

Apply a modified filter to the signal, with +- X seconds from each sample, in order to extract the tonic component. Default is 4 seconds

• **Input:**

- `rawGSRSignal` = gsr signal as list
- `samplerate` = samplerate of the signal
- `seconds` = number of seconds before and after each timepoint to use in order to compute the filtered value

• **Output:**

- tonic signal

**Parameters**

- **rawGSRSignal** (*list*) – raw GSR Signal
- **samplerate** (*int*) – samplerate of the GSR signal in Hz
- **seconds** – seconds to use to apply the phasic filter
- **seconds** – int

**Returns** filtered signal

**Return type** list

### 3.3 Electromyography analysis module

`electromyography.analyzeEMG` (*rawEMGSignal*, *samplerate*, *preprocessing=True*, *lowpass=50*, *highpass=20*, *threshold=0.01*, *nseg=3*, *phasic\_seconds=4*)

This functions acts as entrypoint for the EMG Analysis.

• **Input:**

- `rawEMGSignal` = raw signal as list
- `samplerate` = samplerate of the signal
- `lowpass` = lowpass cutoff in Hz
- `highpass` = highpass cutoff in Hz
- `threshold` for the evaluation of ZC,MYOP,WAMP,SSC
- `nseg` = number of segments for MAVSLPk, MHW,MTW

• **Output:**

- results dictionary

`electromyography.butter_highpass` (*cutoff*, *fs*, *order=5*)

This functions generates a higpass butter filter

**Parameters**

- **cutoff** (*float*) – cutoff frequency
- **cutoff** – cutoff frequency
- **fs** (*float*) – samplerate of the signal

- **order** (*int*) – order of the Butter Filter

**Returns** butter highpass filter

**Return type** list

electromyography.**butter\_highpass\_filter** (*data, cutoff, fs, order*)

This functions apply a butter highpass filter to a signal

**Parameters**

- **data** (*list*) – ECG signal
- **cutoff** (*float*) – cutoff frequency
- **cutoff** – cutoff frequency
- **fs** (*float*) – samplerate of the signal
- **order** (*int*) – order of the Butter Filter

**Returns** highpass filtered ECG signal

**Return type** list

electromyography.**butter\_lowpass** (*cutoff, fs, order=5*)

This functions generates a lowpass butter filter

**Parameters**

- **cutoff** (*float*) – cutoff frequency
- **cutoff** – cutoff frequency
- **fs** (*float*) – samplerate of the signal
- **order** (*int*) – order of the Butter Filter

**Returns** butter lowpass filter

**Return type** list

electromyography.**butter\_lowpass\_filter** (*data, cutoff, fs, order*)

This functions apply a butter lowpass filter to a signal

**Parameters**

- **data** (*list*) – ECG signal
- **cutoff** (*float*) – cutoff frequency
- **cutoff** – cutoff frequency
- **fs** (*float*) – samplerate of the signal
- **order** (*int*) – order of the Butter Filter

**Returns** lowpass filtered ECG signal

**Return type** list

electromyography.**getAAC** (*rawEMGSignal*)

Get the Average amplitude change.:

```
AAC = 1/N * sum(|x(i+1) - xi|) for i = 1 --> N-1
```

• **Input:**

- raw EMG Signal as list

- **Output:**
  - Average amplitude change of the signal

**Parameters** `rawEMGSignal` (*list*) – the raw EMG signal

**Returns** Average Amplitude Change of the signal

**Return type** float

`electromyography.getAFB(rawEMGSignal, samplerate, windowSize=32)`

Get the amplitude at first Burst.

Reference: Du, S., & Vuskovic, M. (2004, November). Temporal vs. spectral approach to feature extraction from prehensile EMG signals. In Information Reuse and Integration, 2004. IRI 2004. Proceedings of the 2004 IEEE International Conference on (pp. 344-350). IEEE.

- **Input:**
  - rawEMGSignal as list
  - samplerate of the signal in Hz (sample / s)
  - windowSize = window size in ms

- **Output:**
  - amplitude at first burst

**Parameters**

- `rawEMGSignal` (*list*) – the raw EMG signal
- `samplerate` (*int*) – samplerate of the signal int Hz
- `windowSize` – window size in ms to use for the analysis

**Returns** Amplitude ad first Burst

**Return type** float

`electromyography.getDASDV(rawEMGSignal)`

Get the standard deviation value of the the wavelength.:

```
DASDV = sqrt( (1 / (N-1)) * sum((x[i+1] - x[i])**2) for i = 1 --> N - 1
```

- **Input:**
  - raw EMG Signal

- **Output:**
  - DASDV

**Parameters** `rawEMGSignal` (*list*) – the raw EMG signal

**Returns** standard deviation value of the the wavelength

**Return type** float

electromyography.**getFR** (*rawEMGPowerSpectrum, frequencies, llc=30, ulc=250, lhc=250, uhc=500*)

This functions evaluate the frequency ratio of the power spectrum.

Cut-off value can be decided experimentally or from the MNF Feature See: Oskoei, M.A., Hu, H. (2006). GA-based feature subset selection for myoelectric classification.

- **Input:**
  - raw EMG power spectrum as list,
  - frequencies as list,
  - llc = lower low cutoff
  - ulc = upper low cutoff
  - lhc = lower high cutoff
  - uhc = upper high cutoff

- **Output:**
  - Frequency Ratio

**Parameters**

- **rawEMGPowerSpectrum** (*list*) – power spectrum of the EMG signal
- **frequencies** (*list*) – frequencies of the PSD
- **llc** (*float*) – lower cutoff frequency for the low frequency components
- **ulc** (*float*) – upper cutoff frequency for the low frequency components
- **lhc** (*float*) – lower cutoff frequency for the high frequency components
- **uhc** (*float*) – upper cutoff frequency for the high frequency components

**Returns** frequencies ratio of the EMG power spectrum

**Return type** float

electromyography.**getHIST** (*rawEMGSignal, nseg=9, threshold=50*)

Histograms is an extension version of ZC and WAMP features.

- **Input:**
  - raw EMG Signal as list
  - nseg = number of segment to analyze
  - threshold = threshold to use to avoid DC fluctuations

- **Output:**
  - get zc/wamp for each segment

**Parameters**

- **rawEMGSignal** (*list*) – the raw EMG signal
- **nseg** (*int*) – number of segments to analyze
- **threshold** (*int*) – value to sum / subtract to the zero when evaluating the crossing.

**Returns** Willison amplitude

**Return type** float

electromyography.**getIEMG**(*rawEMGSignal*)

This function compute the sum of absolute values of EMG signal Amplitude.:

```
IEMG = sum(|xi|) for i = 1 --> N
```

- **Input:**
  - raw EMG Signal as list
- **Output:**
  - integrated EMG

**Parameters** **rawEMGSignal** (*list*) – the raw EMG signal

**Returns** the IEMG of the EMG Signal

**Return type** float

electromyography.**getLOG**(*rawEMGSignal*)

LOG is a feature that provides an estimate of the muscle contraction force.:

```
LOG = e^((1/N) * sum(|xi|)) for x i = 1 --> N
```

- **Input:**
  - raw EMG Signal
- Output = \* LOG

**Parameters** **rawEMGSignal** (*list*) – the raw EMG signal

**Returns** LOG feature of the EMG Signal

**Return type** float

electromyography.**getMAV**(*rawEMGSignal*)

This functions compute the average of EMG signal Amplitude.:

```
MAV = 1/N * sum(|xi|) for i = 1 --> N
```

- **Input:**
  - raw EMG Signal as list
- **Output:**
  - Mean Absolute Value

**Parameters** **rawEMGSignal** (*list*) – the raw EMG signal

**Returns** the MAV of the EMG Signal

**Return type** float

electromyography.**getMAV1**(*rawEMGSignal*)

This functoin evaluate Average of EMG signal Amplitude, using the modified version n°.1.:

```
IEMG = 1/N * sum(wi|xi|) for i = 1 --> N
wi = {
    1 if 0.25N <= i <= 0.75N,
    0.5 otherwise
}
```

- **Input:**
  - raw EMG Signal as list
- **Output:**
  - Mean Absolute Value

**Parameters** `rawEMGSignal` (*list*) – the raw EMG signal

**Returns** the MAV (modified version n. 1) of the EMG Signal

**Return type** float

electromyography.**getMAV2** (*rawEMGSignal*)

This function evaluate Average of EMG signal Amplitude, using the modified version n°.2.:

```
IEMG = 1/N * sum(wi|xi|) for i = 1 --> N
wi = {
    1 if 0.25N <= i <= 0.75N,
    4i/N if i < 0.25N
    4(i-N)/N otherwise
}
```

- **Input:**
  - raw EMG Signal as list
- **Output:**
  - Mean Absolute Value

**Parameters** `rawEMGSignal` (*list*) – the raw EMG signal

**Returns** the MAV (modified version n. 2) of the EMG Signal

**Return type** float

electromyography.**getMAVSLPk** (*rawEMGSignal*, *nseg*)

Mean Absolute value slope is a modified versions of MAV feature.

The MAVs of adjacent segments are determinated.

```
MAVSLPk = MAV[k+1] - MAV[k]; k = 1, ..., k+1
```

- **Input:**
  - raw EMG signal as list
  - nseg = number of segments to evaluate
- **Output:**
  - list of MAVs



**Parameters**

- **rawEMGSignal** (*list*) – the raw EMG signal
- **nseg** (*int*) – number of segments to evaluate

**Returns** Mean absolute slope value

**Return type** float

electromyography.**getMDF** (*rawEMGPowerSpectrum, frequencies*)  
 Obtain the Median Frequency of the PSD.

MDF is a frequency at which the spectrum is divided into two regions with equal amplitude, in other words, MDF is half of TTP feature

- **Input:**
  - raw EMG Power Spectrum
  - frequencies
- **Output:**
  - Median Frequency (Hz)

**Parameters**

- **rawEMGPowerSpectrum** (*list*) – power spectrum of the EMG signal
- **frequencies** (*list*) – frequencies of the PSD

**Returns** median frequency of the EMG power spectrum

**Return type** float

electromyography.**getMNF** (*rawEMGPowerSpectrum, frequencies*)

Obtain the mean frequency of the EMG signal, evaluated as the sum of product of the EMG power spectrum and the frequency divided by total sum of the spectrum intensity:

```
MNF = sum(fPj) / sum(Pj) for j = 1 -> M
M = length of the frequency bin
Pj = power at frequency bin j
fJ = frequency of the spectrum at frequency bin j
```

- **Input:**
  - rawEMGPowerSpectrum: PSD as list
  - frequencies: frequencies of the PSD spectrum as list
- **Output:**
  - Mean Frequency of the PSD

**Parameters**

- **rawEMGPowerSpectrum** (*list*) – power spectrum of the EMG signal
- **frequencies** (*list*) – frequencies of the PSD

**Returns** mean frequency of the EMG power spectrum

**Return type** float

electromyography.**getMNP** (*rawEMGPowerSpectrum*)

This functions evaluate the mean power of the spectrum.:

```
Mean Power = sum(Pj) / M, j = 1 --> M, M = len of the spectrum
```

- **Input:**
  - EMG power spectrum
- **Output:**
  - mean power

**Parameters**

- **rawEMGPowerSpectrum** (*list*) – power spectrum of the EMG signal
- **frequencies** (*list*) – frequencies of the PSD

**Returns** mean power of the EMG power spectrum

**Return type** float

electromyography.**getMYOP** (*rawEMGSignal, threshold*)

The myopulse percentage rate (MYOP) is an average value of myopulse output. It is defined as one absolute value of the EMG signal exceed a pre-defined thershold value.

```
MYOP = (1/N) * sum(|f(xi)|) for i = 1 --> N
f(x) = {
    1 if x >= threshold
    0 otherwise
}
```

- **Input:**
  - rawEMGSignal = EMG signal as list
  - threshold = threshold to avoid fluctuations caused by noise and low voltage fluctuations
- **Output:**
  - Myopulse percentage rate

**Parameters**

- **rawEMGSignal** (*list*) – the raw EMG signal
- **threshold** (*int*) – value to sum / subtract to the zero when evaluating the crossing.

**Returns** Myopulse percentage rate of the signal

**Return type** float

electromyography.**getPSR** (*rawEMGPowerSpectrum, frequencies, n=20, fmin=10, fmax=500*)

This function computes the Power Spectrum Ratio of the signal, defined as: Ratio between the energy P0 which is nearby the maximum value of the EMG power spectrum and the energy P which is the whole energy of the EMG power spectrum

- **Input:**
  - EMG power spectrum
  - frequencies as list

- n = range around f0 to evaluate P0
- fmin = min frequency
- fmax = max frequency

**Parameters**

- **rawEMGPowerSpectrum** (*list*) – power spectrum of the EMG signal
- **frequencies** (*list*) – frequencies of the PSD
- **n** (*int*) – range of frequencies around f0 to evaluate
- **fmin** (*int*) – min frequency to evaluate
- **fmax** (*int*) – lmaximum frequency to evaluate

**Returns** Power spectrum ratio of the EMG power spectrum

**Return type** float

`electromyography.getPeakFrequency` (*rawEMGPowerSpectrum, frequencies*)

Obtain the frequency at which the maximum peak occur

• **Input:**

- raw EMG Power Spectrum as list
- frequencies as list

• **Output:**

- frequency in Hz

**Parameters**

- **rawEMGPowerSpectrum** (*list*) – power spectrum of the EMG signal
- **frequencies** (*list*) – frequencies of the PSD

**Returns** peakfrequency of the EMG Power spectrum

**Return type** float

`electromyography.getRMS` (*rawEMGSignal*)

Get the root mean square of a signal.:

$$RMS = (\text{sqrt}((1 / N) * \text{sum}(xi**2))) \text{ for } i = 1 \text{ --> } N$$

• **Input:**

- raw EMG Signal as list

• **Output:**

- Root mean square of the signal

**Parameters** **rawEMGSignal** (*list*) – the raw EMG signal

**Returns** Root mean square of the EMG signal

**Return type** float

electromyography.**getSM**(*rawEMGPowerSpectrum, frequencies, order*)

Get the spectral moment of a spectrum:

```
SM = sum(fj*(Pj**order)), j = 1 --> M
```

• **Input:**

- raw EMG Power Spectrum
- frequencies as list
- order (int)

• **Output:**

- SM of order = order

**Parameters**

- **rawEMGPowerSpectrum** (*list*) – power spectrum of the EMG signal
- **frequencies** (*list*) – frequencies of the PSD
- **order** (*int*) – order to the moment

**Returns** Spectral moment of order X of the EMG power spectrum

**Return type** float

electromyography.**getSSC**(*rawEMGSignal, threshold*)

Number of times the slope of the EMG signal changes sign.:

```
SSC = sum(f( (x[i] - x[i-1]) X (x[i] - x[i+1]))) for i = 2 --> n-1

f(x) {
  1 if x >= threshold
  0 otherwise
}
```

• **Input:**

- raw EMG Signal

• **Output:**

- number of Slope Changes

**Parameters**

- **rawEMGSignal** (*list*) – the raw EMG signal
- **threshold** (*int*) – value to sum / subtract to the zero when evaluating the crossing.

**Returns** Number of slope's sign changes

**Return type** int

electromyography.**getSSI**(*rawEMGSignal*)

This function compute the summation of square values of the EMG signal.:

```
SSI = sum(xi**2) for i = 1 --> N
```

- **Input:**
  - raw EMG Signal as list
- **Output:**
  - Simple Square Integral

**Parameters** `rawEMGSignal` (*list*) – the raw EMG signal

**Returns** SSI of the signal

**Return type** float

`electromyography.getTM` (*rawEMGSignal*, *order*)

This function compute the Temporal Moment of order X of the EMG signal.:

$$TM = (1 / N * \sum(xi^{**order}) \text{ for } i = 1 \text{ --> } N$$

- **Input:**
  - raw EMG Signal as list
- **Output:**
  - TM of order = order

**Parameters**

- `rawEMGSignal` (*list*) – the raw EMG signal
- `order` (*int*) – order the the TM function

**Returns** Temporal Moment of order X of the EMG signal

**Return type** float

`electromyography.getTTP` (*rawEMGPowerSpectrum*)

This functions evaluate the aggregate of the EMG power spectrum (aka Zero Spectral Moment)

- **Input:**
  - raw EMG Power Spectrum
- **Output:**
  - Total Power

**Parameters**

- `rawEMGPowerSpectrum` (*list*) – power spectrum of the EMG signal
- `frequencies` (*list*) – frequencies of the PSD

**Returns** total power of the EMG power spectrum

**Return type** float

`electromyography.getVAR` (*rawEMGSignal*)

Summation of average square values of the deviation of a variable.:

$$VAR = (1 / (N - 1)) * \sum(xi^{**2}) \text{ for } i = 1 \text{ --> } N$$

- **Input:**
  - raw EMG Signal as list
- **Output:**
  - Summation of the average square values

**Parameters** `rawEMGSignal` (*list*) – the raw EMG signal

**Returns** the VAR of the EMG Signal

**Return type** float

`electromyography.getVCF(SM0, SM1, SM2)`

This function evaluate the variance of the central frequency of the PSD.:

$$VCF = (1 / SM0) * \sum (P_j * (f_j - f_c) ** 2), j = 1 \rightarrow M, = SM2 / SM0 - (SM1 / SM0) ** 2$$

- **Input:**
  - SM0: spectral moment of order 0
  - SM1: spectral moment of order 1
  - SM2: spectral moment of order 0
- **Output:**
  - Variance of Central frequency of the Power spectrum

**Parameters**

- **SM0** (*float*) – Spectral moment of order 0
- **SM1** (*float*) – Spectral moment of order 1
- **SM2** (*float*) – Spectral moment of order 2

**Returns** Variance of central frequency

**Return type** float

`electromyography.getWAMP(rawEMGSignal, threshold)`

Wilson or Willison amplitude is a measure of frequency information. It is a number of time resulting from difference between the EMG signal of two adjoining segments, that exceed a threshold.:

```
WAMP = sum( f(|x[i] - x[i+1]|)) for n = 1 --> n-1
f(x) {
    1 if x >= threshold
    0 otherwise
}
```

- **Input:**
  - rawEMGSignal = EMG signal as list
  - threshold = threshold to avoid fluctuations caused by noise and low voltage fluctuations
- **Output:**
  - Wilson Amplitude value

**Parameters**

- **rawEMGSignal** (*list*) – the raw EMG signal
- **threshold** (*int*) – value to sum / subtract to the zero when evaluating the crossing.

**Returns** Willison amplitude

**Return type** float

electromyography.**getWL** (*rawEMGSignal*)

Get the waveform length of the signal, a measure of complexity of the EMG Signal.:

```
WL = sum(|x(i+1) - xi|) for i = 1 --> N-1
```

• **Input:**

- raw EMG Signal as list

• **Output:**

- wavelength of the signal

**Parameters** **rawEMGSignal** (*list*) – the raw EMG signal

**Returns** Waveform length of the signal

**Return type** float

electromyography.**getZC** (*rawEMGSignal, threshold*)

How many times does the signal crosses the 0 (+-threshold):

```
ZC = sum([sgn(x[i] X x[i+1]) intersected |x[i] - x[i+1]| >= threshold]) for i = 1 --> N - 1
sign(x) = {
    1, if x >= threshold
    0, otherwise
}
```

• **Input:**

- rawEMGSignal = EMG signal as list
- threshold = threshold to use in order to avoid fluctuations caused by noise and low voltage fluctuations

• **Output:**

- ZC index

**Parameters**

- **rawEMGSignal** (*list*) – the raw EMG signal
- **threshold** (*int*) – value to sum / subtract to the zero when evaluating the crossing.

**Returns** Number of times the signal crosses the 0 (+- threshold)

**Return type** float

electromyography.**phasicFilter** (*rawEMGSignal, samplerate, seconds=4*)

Apply a phasic filter to the signal, with +-4 seconds from each sample

- **Input:**
  - rawEMGSignal = emg signal as list
  - samplerate = samplerate of the signal

- **Output:**
  - phasic filtered signal

**Parameters**

- **rawEMGSignal** (*list*) – the raw EMG signal
- **samplerate** (*int*) – samplerate of the signal in Hz

**Returns** the phasic filtered signal

**Return type** list



# CHAPTER 4

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## Tutorials

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Quickstart v.0.0.9



## CHAPTER 5

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Cite

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If you use PySiology in your work, please cite:

Gabrieli G., Azhari A., Esposito G. (2020) PySiology: A Python Package **for**  
↳ Physiological Feature Extraction. In: Esposito A., Faundez-Zanuy M., Morabito F.,  
↳ Pasero E. (eds) Neural Approaches to Dynamics of Signal Exchanges. Smart Innovation,  
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## 6.1 Articles

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3. Valderas, M. T., Bolea, J., Laguna, P., Vallverdú, M., & Bailón, R. (2015, August). Human emotion recognition using heart rate variability analysis with spectral bands based on respiration. In *Engineering in Medicine and Biology Society (EMBC), 2015 37th Annual International Conference of the IEEE* (pp. 6134-6137). IEEE.
4. Ferdinando, H., Seppänen, T., & Alasaarela, E. (2016, October). Comparing features from ECG pattern and HRV analysis for emotion recognition system. In *Computational Intelligence in Bioinformatics and Computational Biology (CIBCB), 2016 IEEE Conference on* (pp. 1-6). IEEE.

### 6.1.2 EDA

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### **6.1.3 EMG**

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4. Künecke, J., Hildebrandt, A., Recio, G., Sommer, W., & Wilhelm, O. (2014). Facial EMG responses to emotional expressions are related to emotion perception ability. *PloS one*, 9(1), e84053.

## **6.2 Websites**

- <http://www.paulvangent.com>

## **6.3 Other resources**

1. GSR Everything you need to know about Galvanic Skin Response to push your insights into emotional behavior, iMotions

## CHAPTER 7

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